

# PD233: Design of Biomedical Devices and Systems

(Lecture-8 Medical Imaging Systems)  
(Imaging Systems Basics, X-ray and CT)

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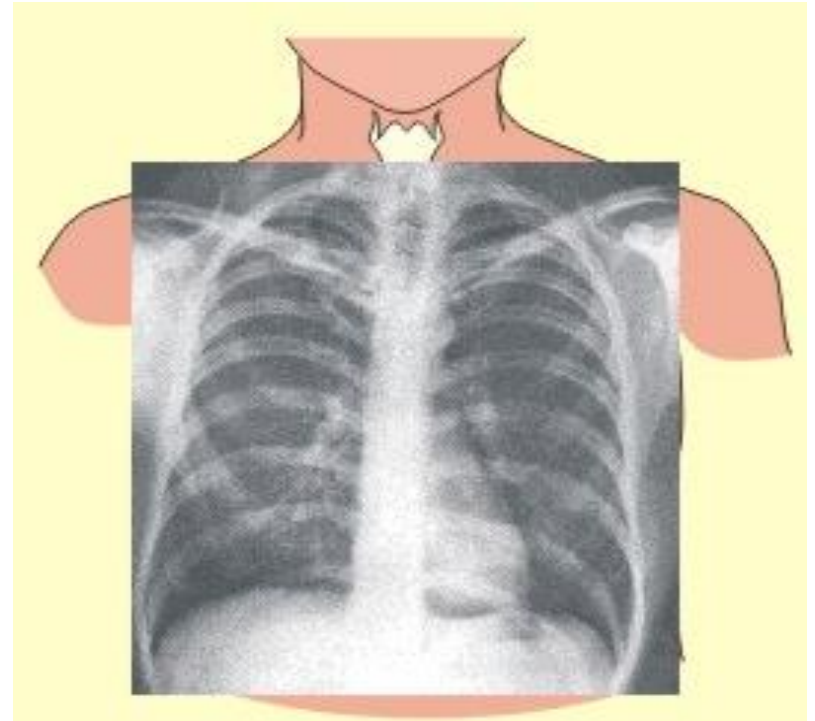
CPDM, IISc

Course Website:

<http://cpdm.iisc.ac.in/utsaah/courses/>

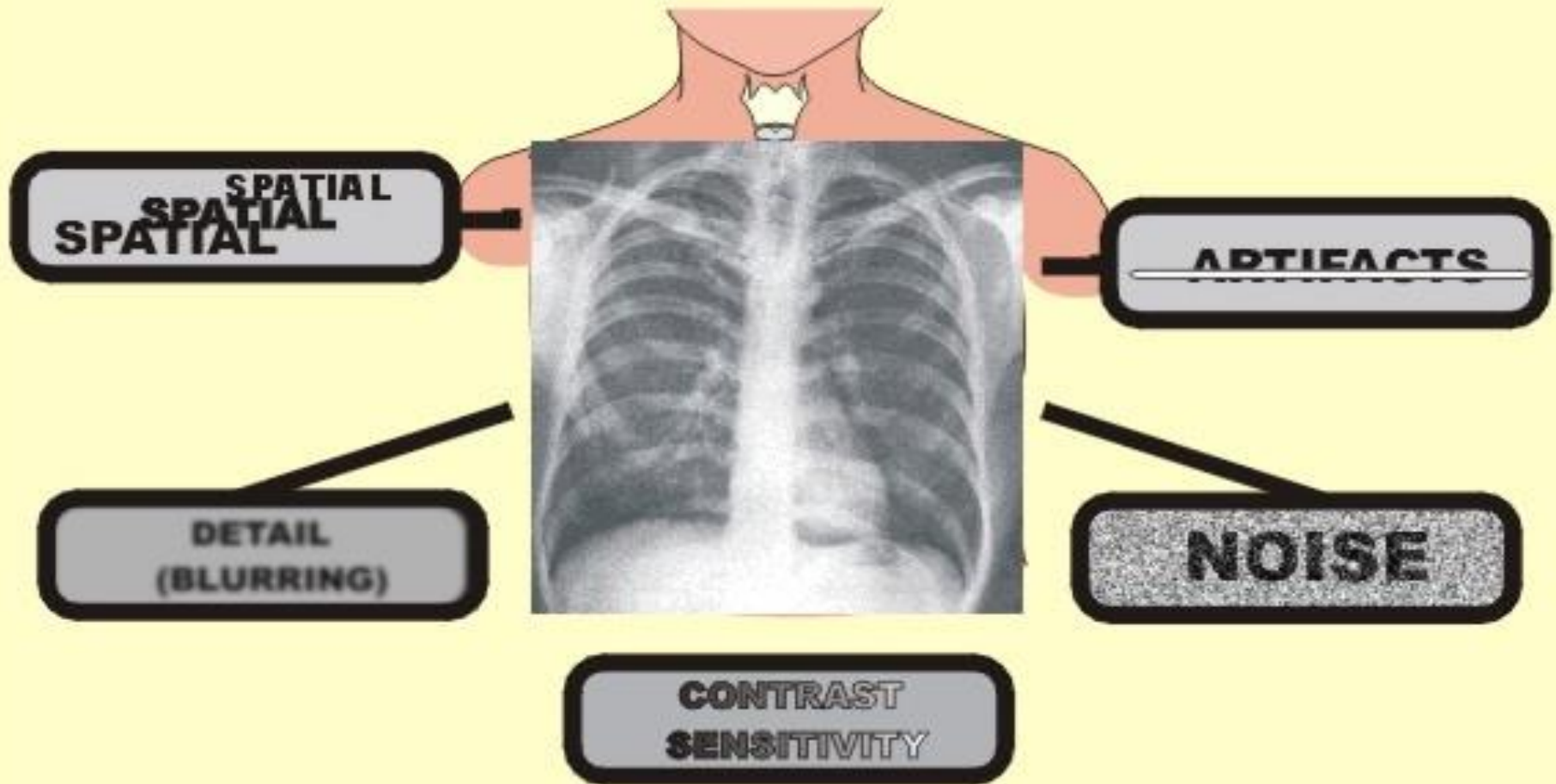
# Medical Imaging Systems

- X- ray
- Computed Tomography (CT)
- Magnetic Resonance Imaging (MRI)
- Ultrasound (US)
- Photoacoustics (PA)
- Optical Coherence Tomography (OCT)



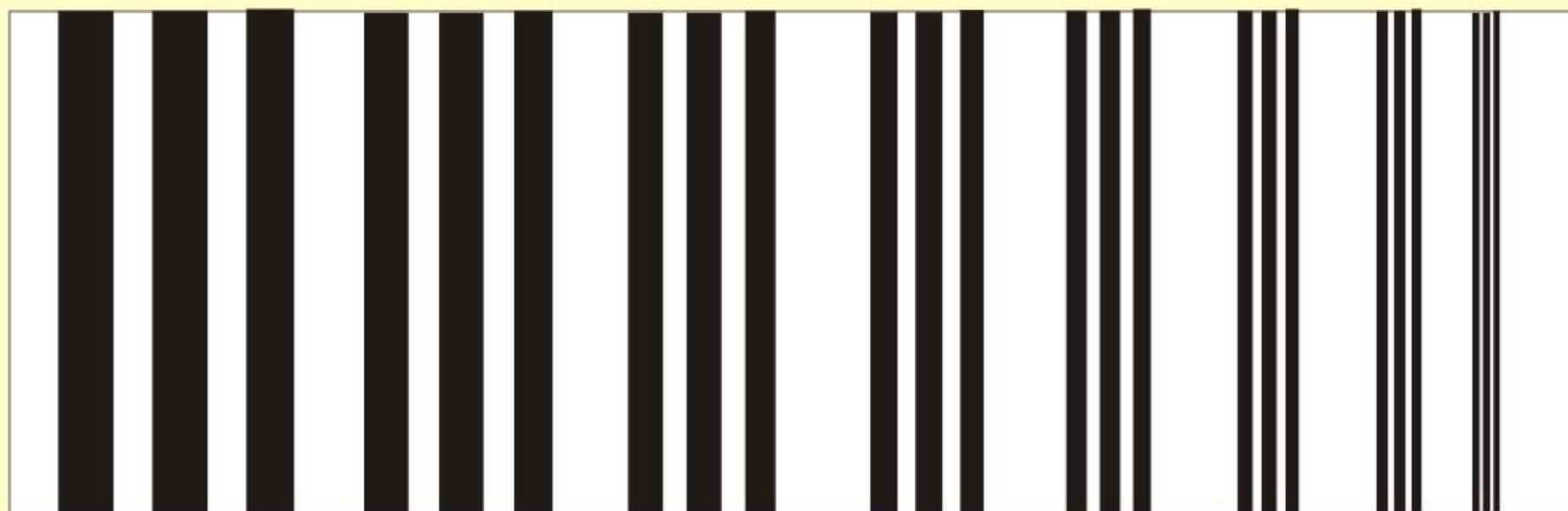
- Provide a window into the body to see ***anatomy*** and ***signs of pathology***
- No window is perfect

# IMAGE QUALITY CHARACTERISTICS



**THAT AFFECT VISIBILITY**

# RESOLUTION TEST PATTERN

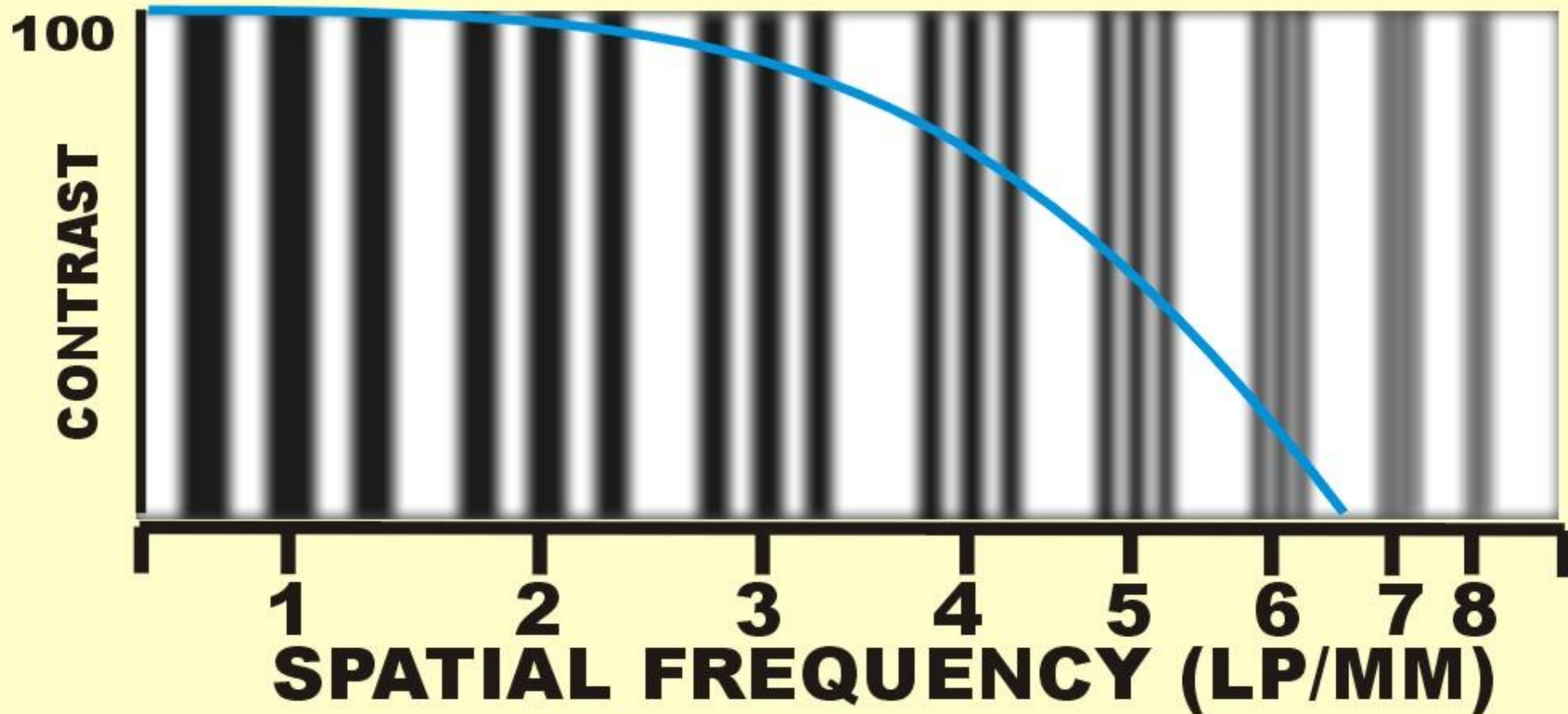


1 2 3 4 5 6 7 8  
**SPATIAL FREQUENCY (LP/MM)**

*Sprawls*

# CONTRAST TRANSFER FUNCTION

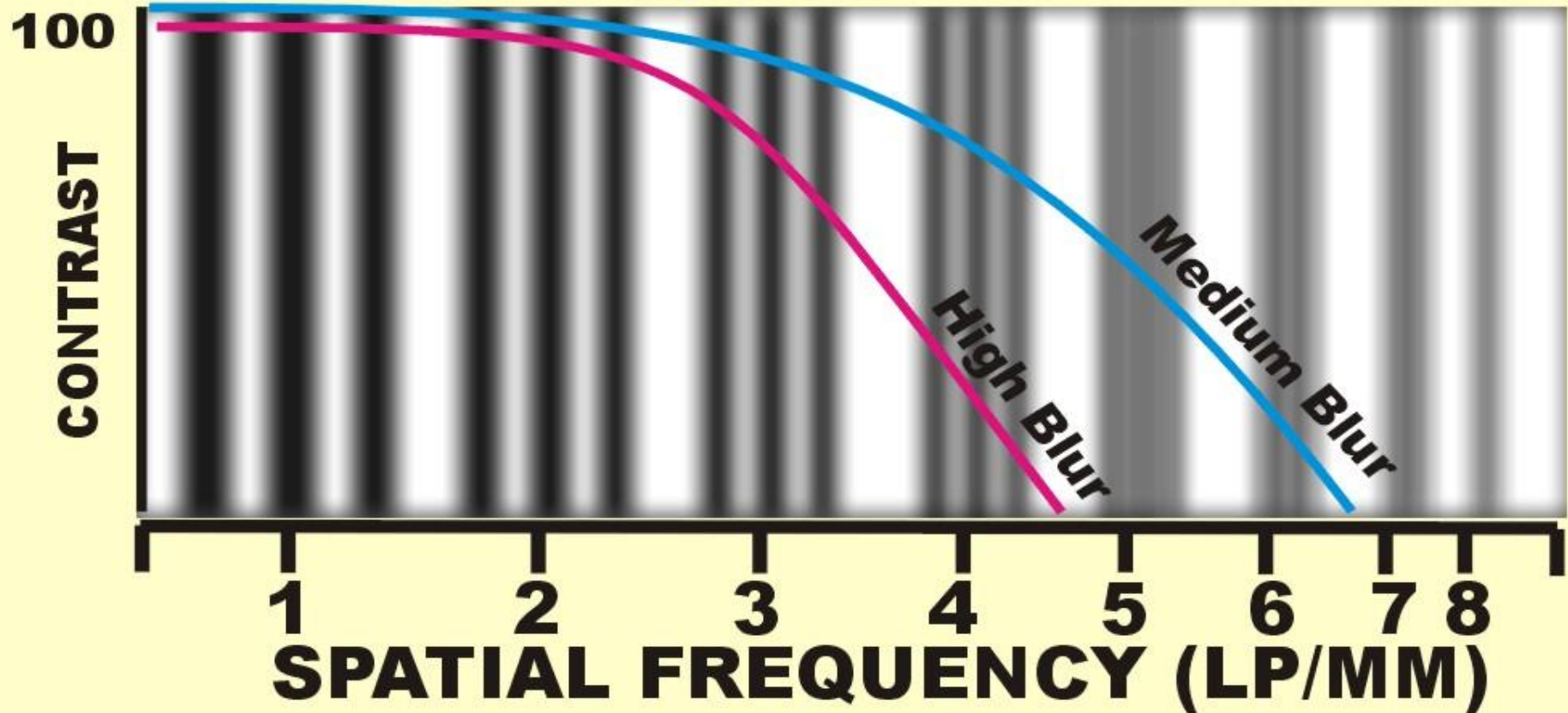
Medium Blur



*Sprawls*

# CONTRAST TRANSFER FUNCTION

High Blur



*Sprawls*



# Accuracy of Diagnostic System

Clinical questions:

- Is the bone fractured?
- Is a kidney stone present?
- Is there a blockage in the artery?

		Disease Present	
		+	-
Diagnostic Test Result	+	<b>a</b> True Positive	<b>b</b> False Positive
	-	<b>c</b> False Negative	<b>d</b> True Negative

Sensitivity →

Probability of positive test given patient is sick

$$TP / (TP + FN)$$

Specificity → the extent to which a diagnostic test is specific for a particular condition,

Probability of negative test given patient is well

$$TN / (TN + FP)$$

accuracy?

# Accuracy of Diagnostic System

Positive Predictive Value:

If the test is positive what is the probability what is the probability that the disease is present.

Negative Predictive Value:

If the test is negative what is the probability what is the probability that the disease is absent.

		Disease Present	
		+	-
Imaging Test Result	+	a	b
	-	c	d

Prevalence: Fraction of population with diseases present in a given population at a given time



# X-Ray Imaging



"First medical X-ray by Wilhelm Röntgen of his wife Anna Bertha Ludwig's hand " by Wilhelm Röntgen.

Reading material: Chapter 1, Kirk Shung

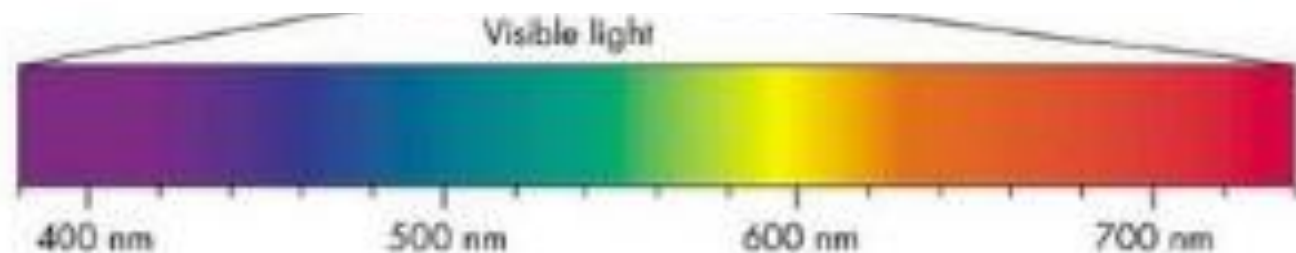
# Electromagnetic (EM) wave Spectrum

$$\frac{\partial^2 E}{\partial x^2} = \frac{1}{c^2} \frac{\partial^2 E}{\partial t^2} \quad \text{and} \quad \frac{\partial^2 B}{\partial x^2} = \frac{1}{c^2} \frac{\partial^2 B}{\partial t^2}$$

for the electric Field

for the magnetic Field

$$\text{where } \frac{1}{c^2} = \epsilon_0 \mu_0$$



# X-Ray as Particle

Energy of a single photon

$$E = hf$$

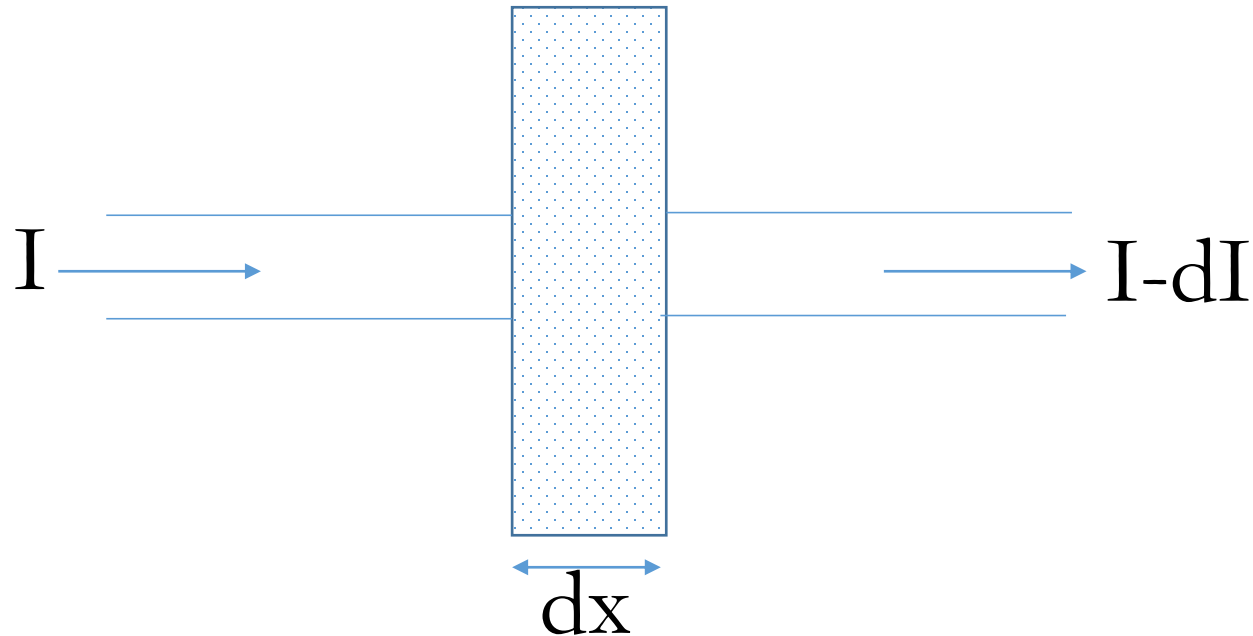
$h$  = Plancks Constant

$$= 4.13 \times 10^{-18} \text{ keV-sec}$$

What is eV?

Calculate energy of single 1nm X-ray Photon

# Attenuation of X-Ray beam



Beam of intensity  $I$  and cross-sectional area  $A$

$$dI = -\beta I dx$$

$\beta$  = Linear attenuation coefficient

**At what distance will the Intensity become half?**

**What will happen if material changes state/density?**

# Attenuation of X-Ray beam

$$\text{Half Layer Value} = 0.693/\beta$$

<b><i>Material</i></b>	<b><i>HVL (mm)</i></b>		
	<b><i>30 keV</i></b>	<b><i>60 keV</i></b>	<b><i>120 keV</i></b>
<b>Tissue</b>	20.0	35.0	45.0
<b>Aluminum</b>	2.3	9.3	16.6
<b>Lead</b>	0.02	0.13	0.15

$$\text{Mass-attenuation coefficient} = \beta/\rho$$

$\rho$  =density

$$\beta = n\sigma$$

Material has **n** atoms per unit volume each with cross section  **$\sigma$**

## Intensity of X-ray beam

Intensity  $\propto$  energy of the photons  
 $\propto$  number of photons

**X-Ray Dose** –should also account for time of exposure

**Roentgen (R):** total number of ions produced in 1cc of air at (760mm Hg and 0°C)

**Radiation Absorbed Dose(rad):** X-Ray energy absorbed per kg of material

$$1\text{rad} = 0.01 \text{ Joules absorbed per kg}$$

$$1 \text{ gray (Gy)} = 100 \text{ rad}$$

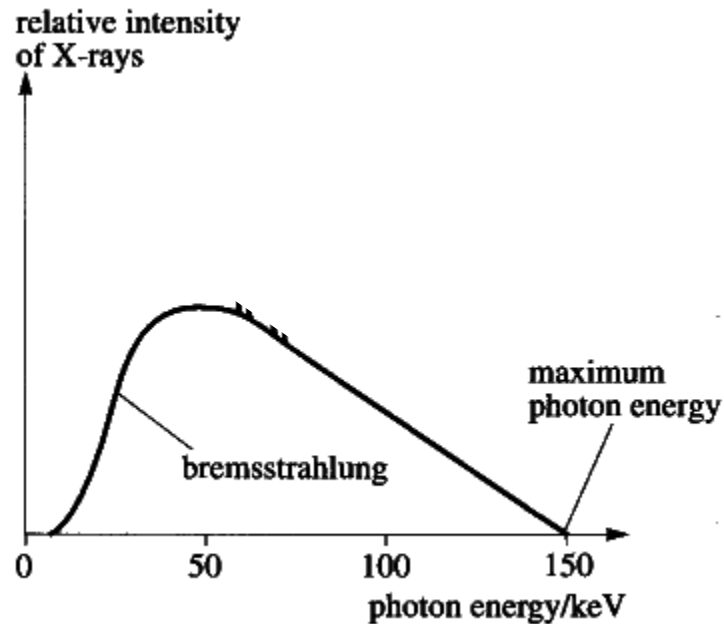
# X-ray Generation

**X –Rays can be generated by bombarding metal targets with high energy electron**

## **White Radiation:**

Energy lost by striking electron interact with the positivity charged metal targets inelastically

Also know as Bremsstrahlung or stopping radiation



## **Characteristic Radiation:**

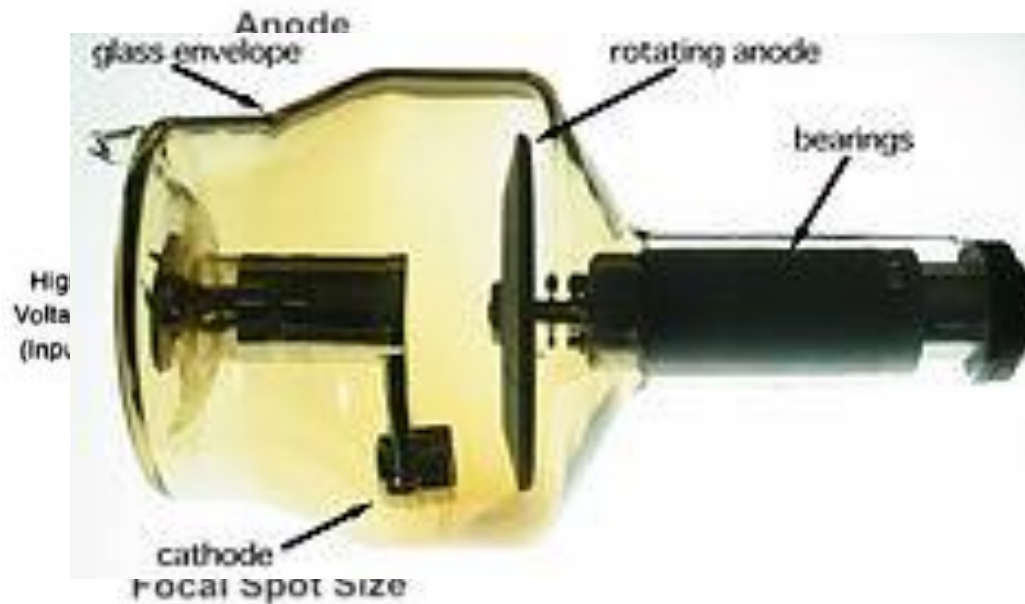
When inner shell electrons are removed by interaction striking electrons

This phenomenon similar to photoelectric effect



# X-ray Generators

X –Rays can be generated by bombarding metal targets with high energy electron



## X ray Tube Characteristics

- Target material
- Tube voltage
- Tube current
- Filament current

Striking electrons heat up  
the metal target

## Line Focus Principle

Large focal spot on the surface but  
small effective spot

$$F = f \sin(\theta)$$

## Rotating Anode

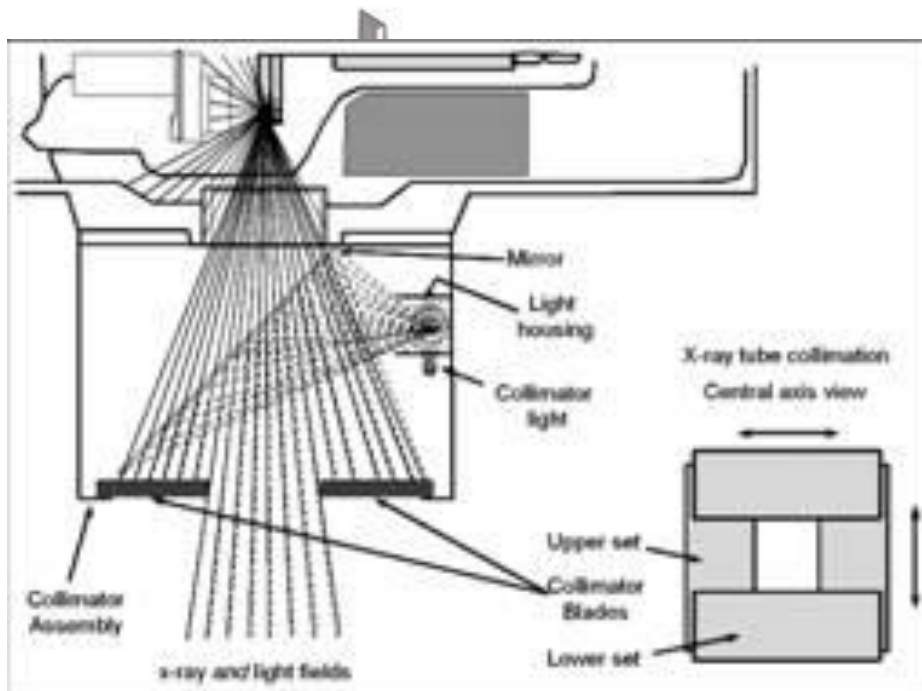
3000 to 10000 rpm

# Beam Restrictors

Needed to regulate size and shape of the x-ray beam

## Beam Restrictors:

- Aperture diaphragms
- Cone and cylinders
- Collimators

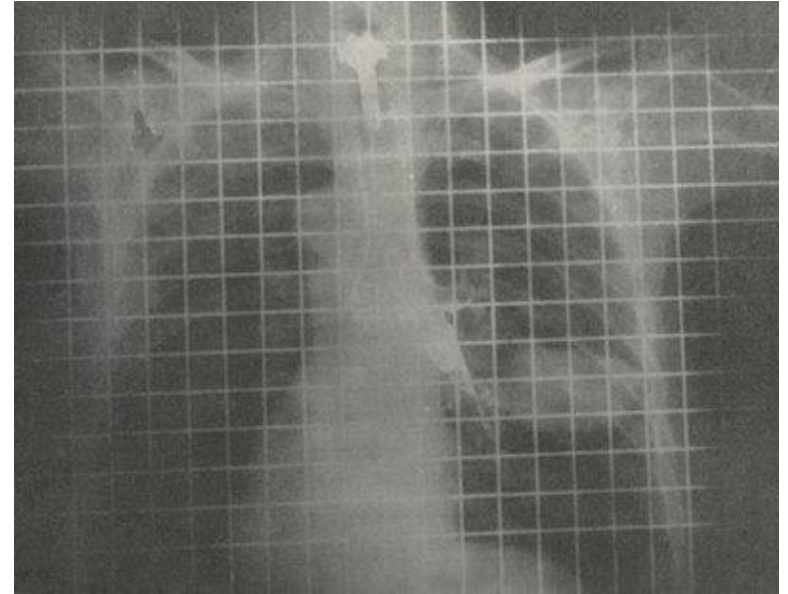
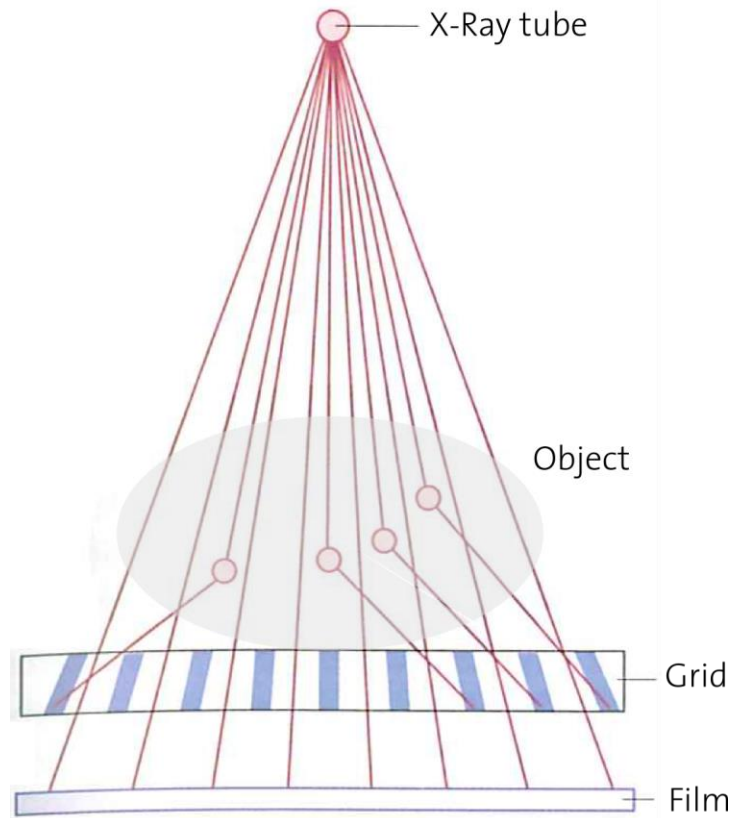


Collimators provide moveable opening  
Light used as a guide to see the region to be exposed by x-ray

Note Finite focal spot leads to penumbra along edges

# Grids

Used to remove effect scattered emissions



Early image of x-ray with grid



Snap on grid, attaches to the x-ray film cassette

# X-ray Detectors

## X-Ray (Photographic) films

X-Ray produces free electrons, which reduces silver halide in the exposed region

Silver halide is black, hence region less exposed appear bright

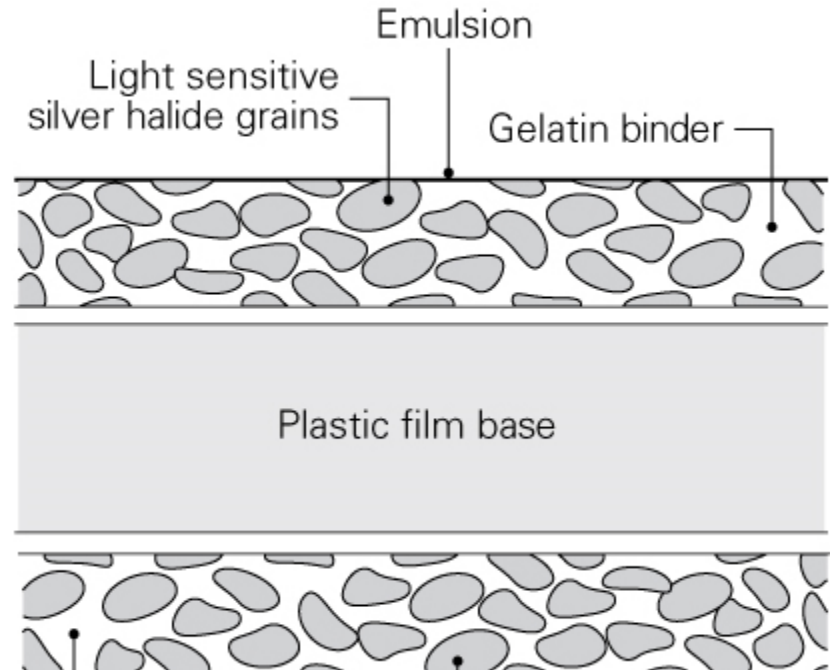
## Digital Radiography (DR)

Uses reversible chemistry

Exposed film is scanned by variety of means

-camera, drum scanner, laser scanning

Alternatively, x ray detectors can be electronics/digitals



Self study!

X Ray film characteristics

response curve, speed, fog, speed

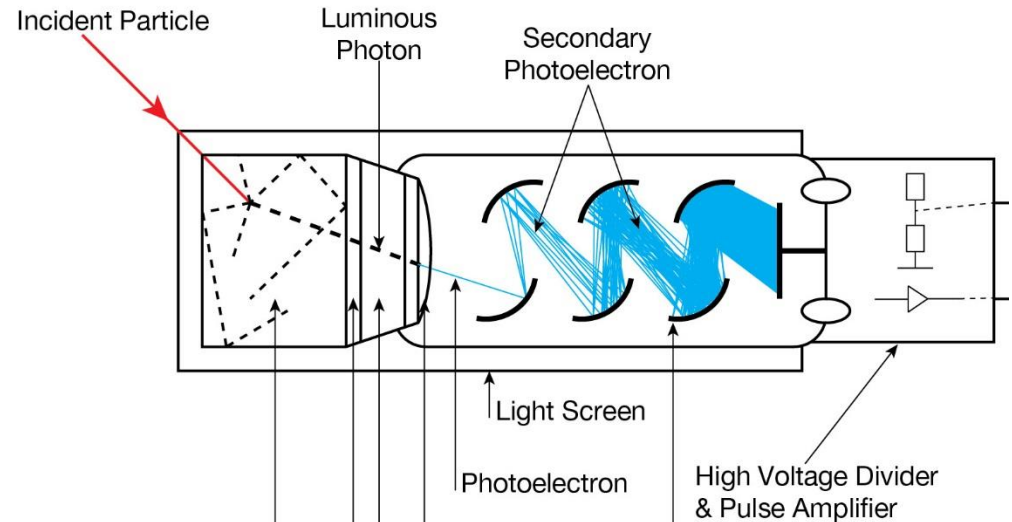
# X-ray Detectors

## Scintillation Detectors

X-Ray photon can produce visible photon in scintillation material (NaI, Th)

Visible photons are amplified by photomultiplier tube (PMT)

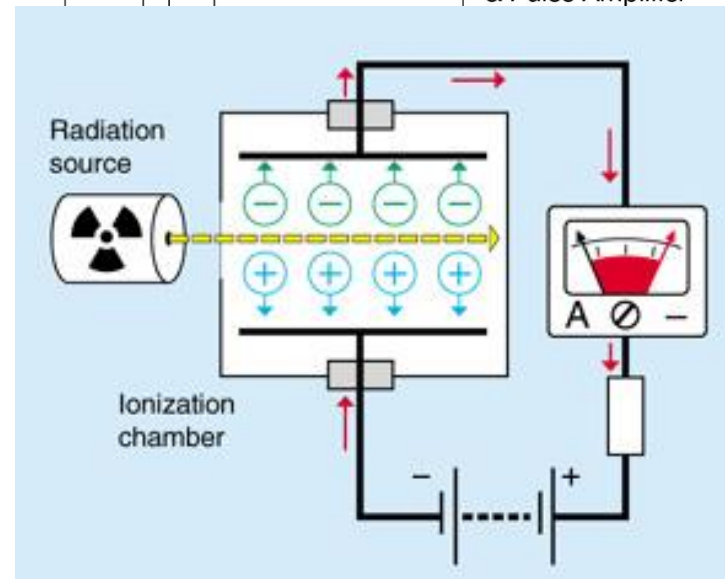
-85% efficient



## Ionization Chamber Detectors

X Ray ionizes inert gases in confined chamber placed between charged electrodes.

Amount of ions produced result in a current which is digitized



# Limitation of Conventional X-ray imaging

- 1) 2d Projection of 3D object – i.e. multiple planes are mapped on to one plane – depth information is lost
- 2) Limited use to distinguish soft tissue
- 3) Conventional X ray is not quantitative
  - Image intensity/size depend on source-object-detectors distance

# Biological Effects of X-Ray

Factors effecting biological effects:

## **Threshold:**

Quantitative level above which there is an tissue damage happens

## **Exposure Time:**

## **Exposure Area:**

## **Biological Variation:**

Response varies from varies from species to species, tissue to tissue

Lethal dose vs short term effects



# Biological Effects of X-Ray

LD 50/30:

Dose of substance or radiation which will kill 50% of the individual over a 30 day period.

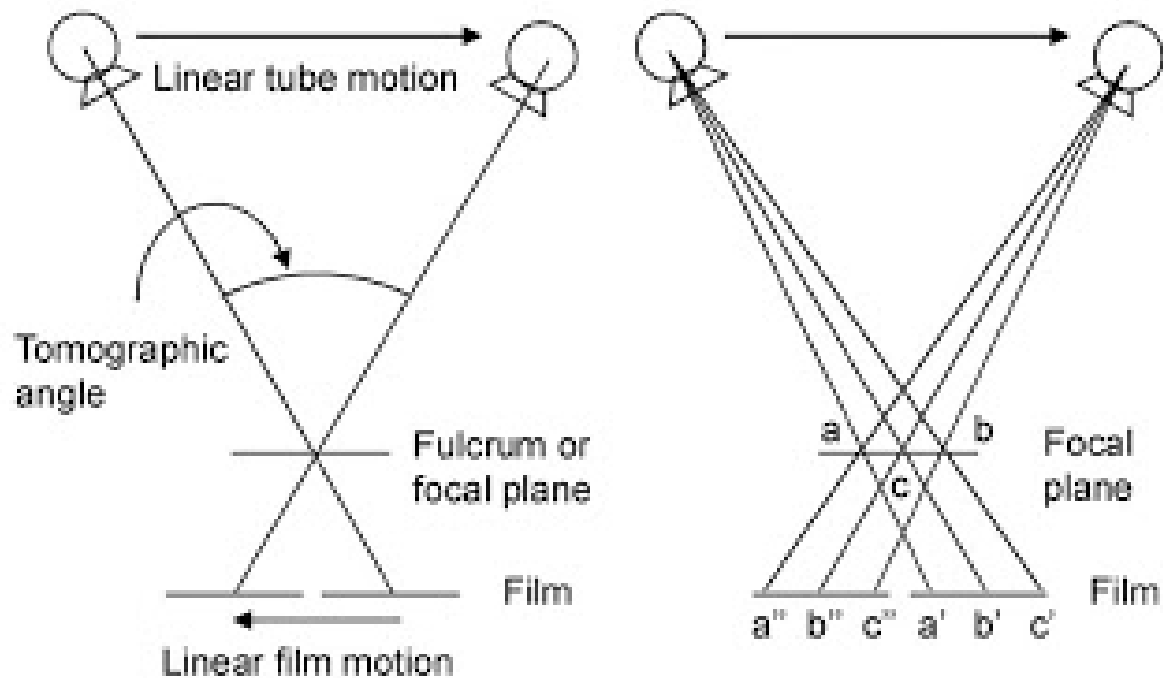
Lethal dose for humans is  $\sim 450$  rad

Short term effects like nausea, vomiting can happen at dose of 100rad

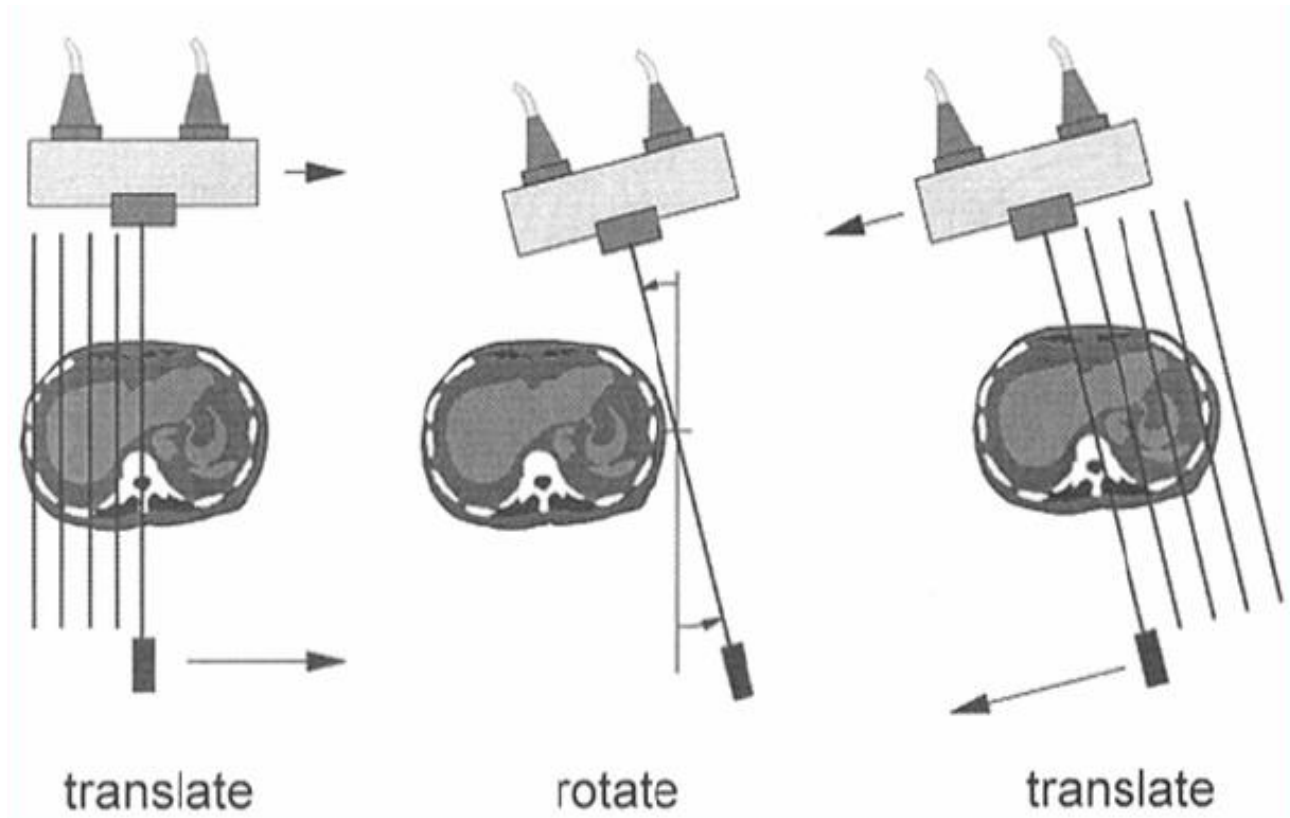
- + carcinogenic effects
- + genetic effects

Even diagnostic X ray is harmful!!

# Conventional Tomography



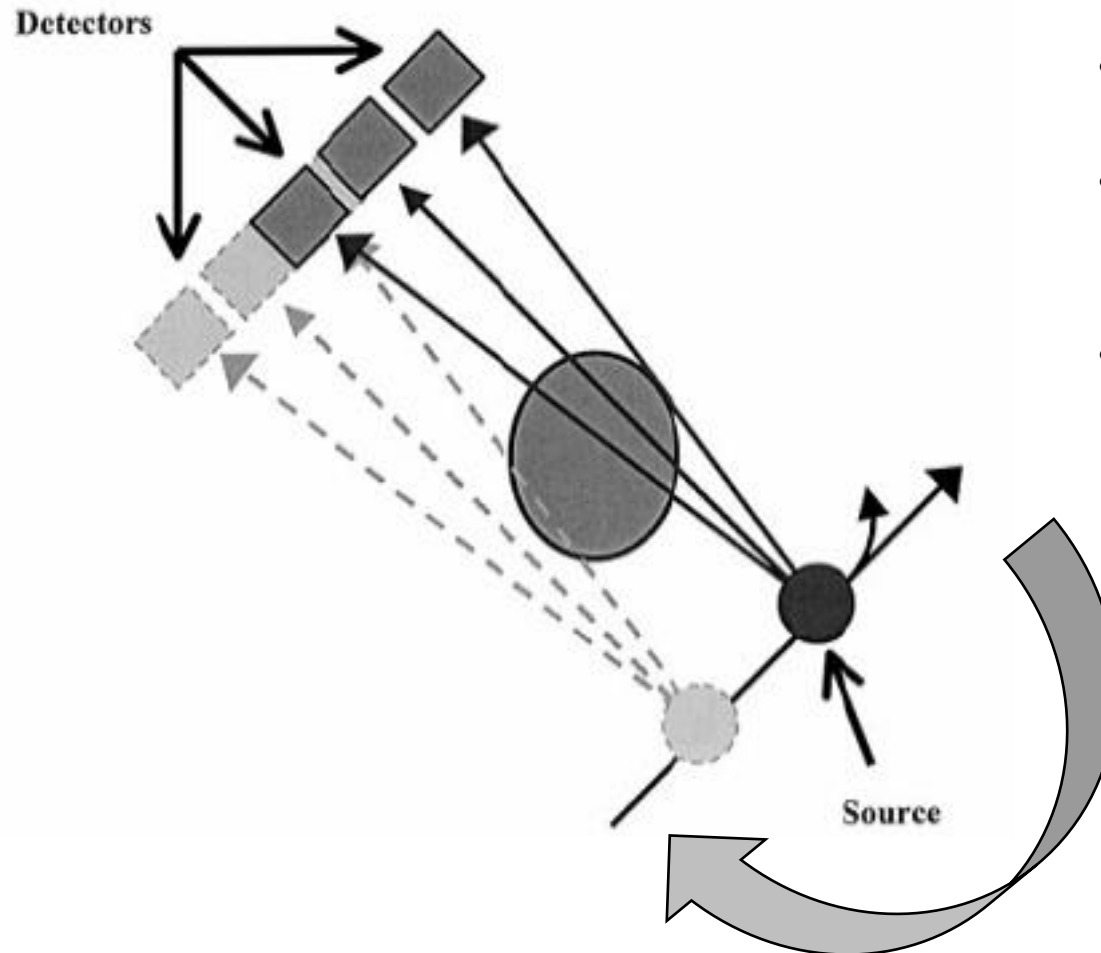
# 1<sup>st</sup> Gen. Computed Tomography



- Few minutes for each scan
- Pencil beams

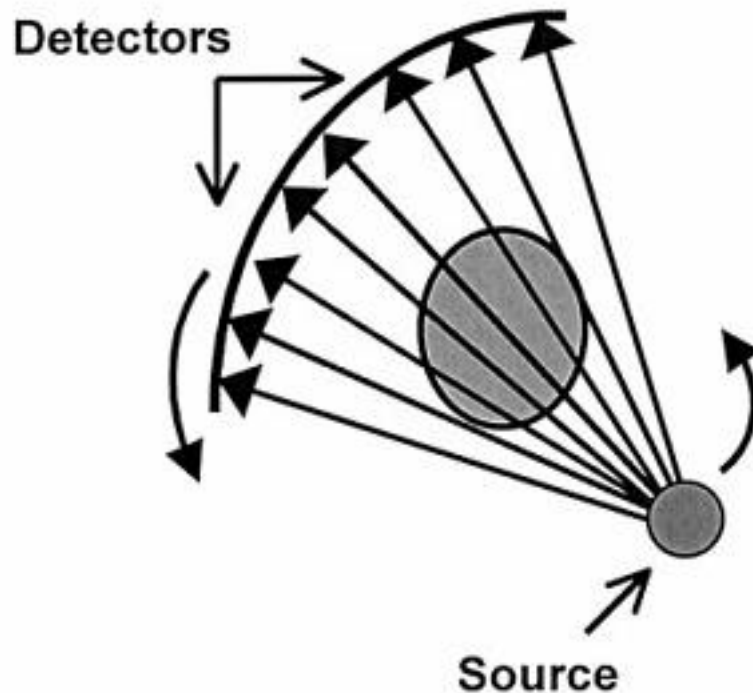
- Motion artifacts
- Translate and Rotate Scanner

# 2<sup>st</sup> Gen. Computed Tomography



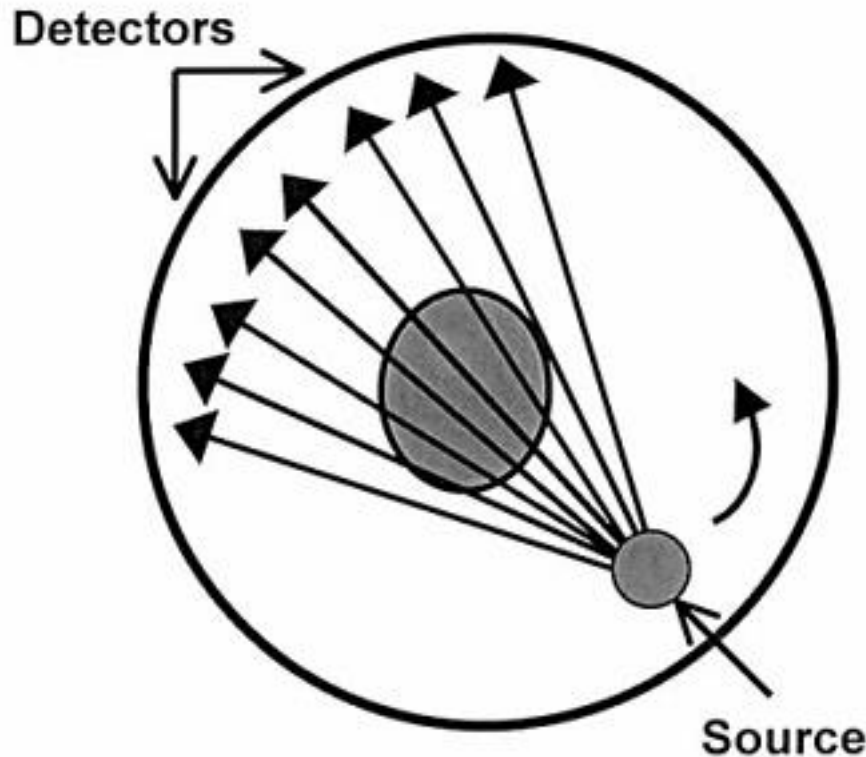
- Multiple detector for single beam
- Initial versions with 3 detectors later upto 50+ detectors
- Still uses translate and rotate scanner

# 3<sup>rd</sup> Gen. Computed Tomography

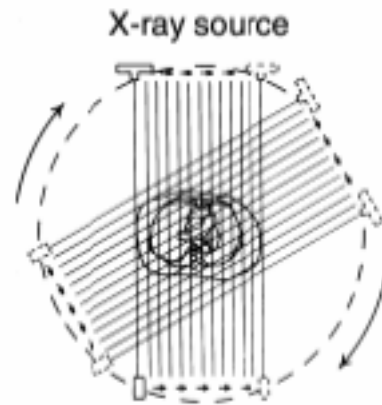


- 300-500 detectors
- Designed for pure rotational scanning
- X ray tube collimated for fan-beam
- Scanning time reduced to 2 sec per slice
- Got rid of translate and rotate scanning – even used in most recent configurations

# 4<sup>th</sup> Gen. Computed Tomography

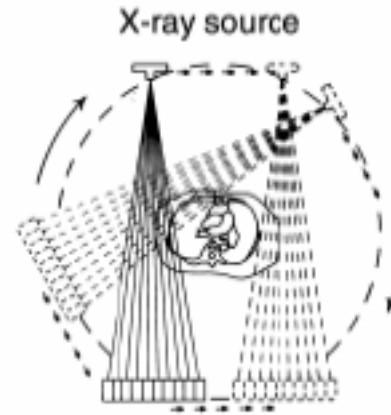


- Circular array of fixed detectors
- Only source rotates
- 600-4800 detectors
- Less efficient as only  $\frac{1}{4}$  of detectors used at any point in time.



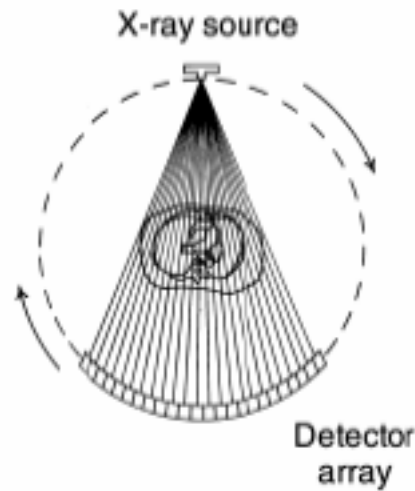
Single detector

1<sup>st</sup> generation CT scanner  
(Parallel beam,  
translate-rotate)



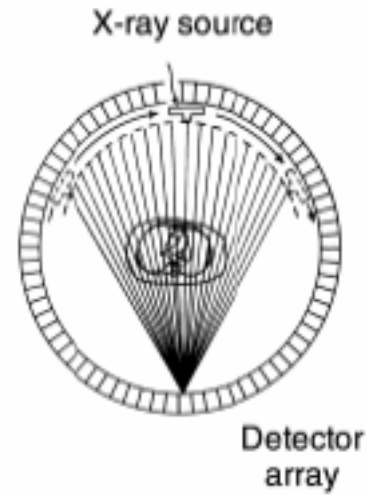
Detector array

2<sup>nd</sup> generation CT scanner  
(Fan beam, translate-rotate)



Detector  
array

3<sup>rd</sup> generation CT scanner  
(Fan beam, rotate only)



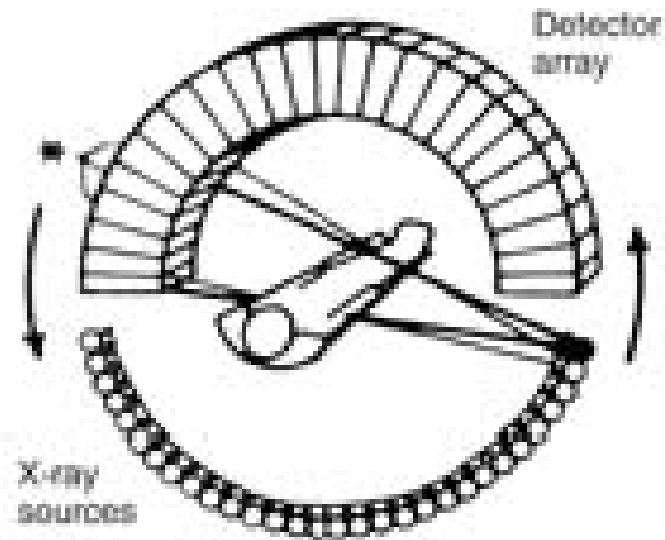
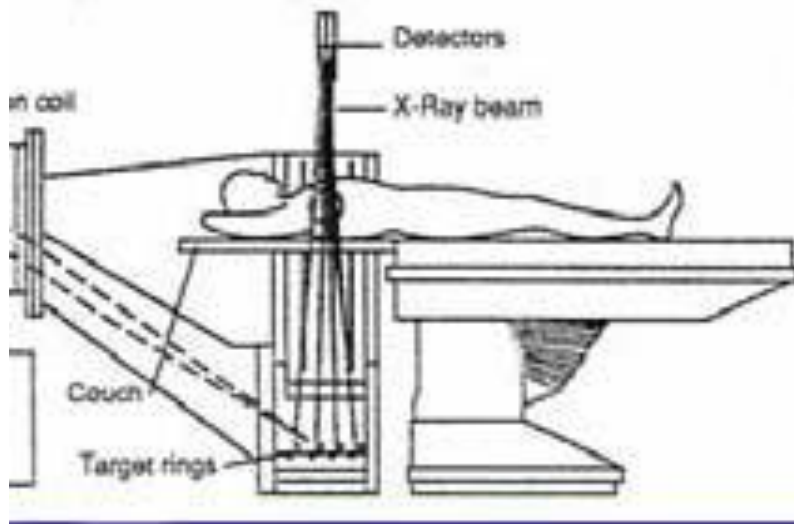
Detector  
array

4<sup>th</sup> generation CT scanner  
(Fan beam, stationary  
circular detector)



# 5<sup>th</sup> Gen. Computed Tomography

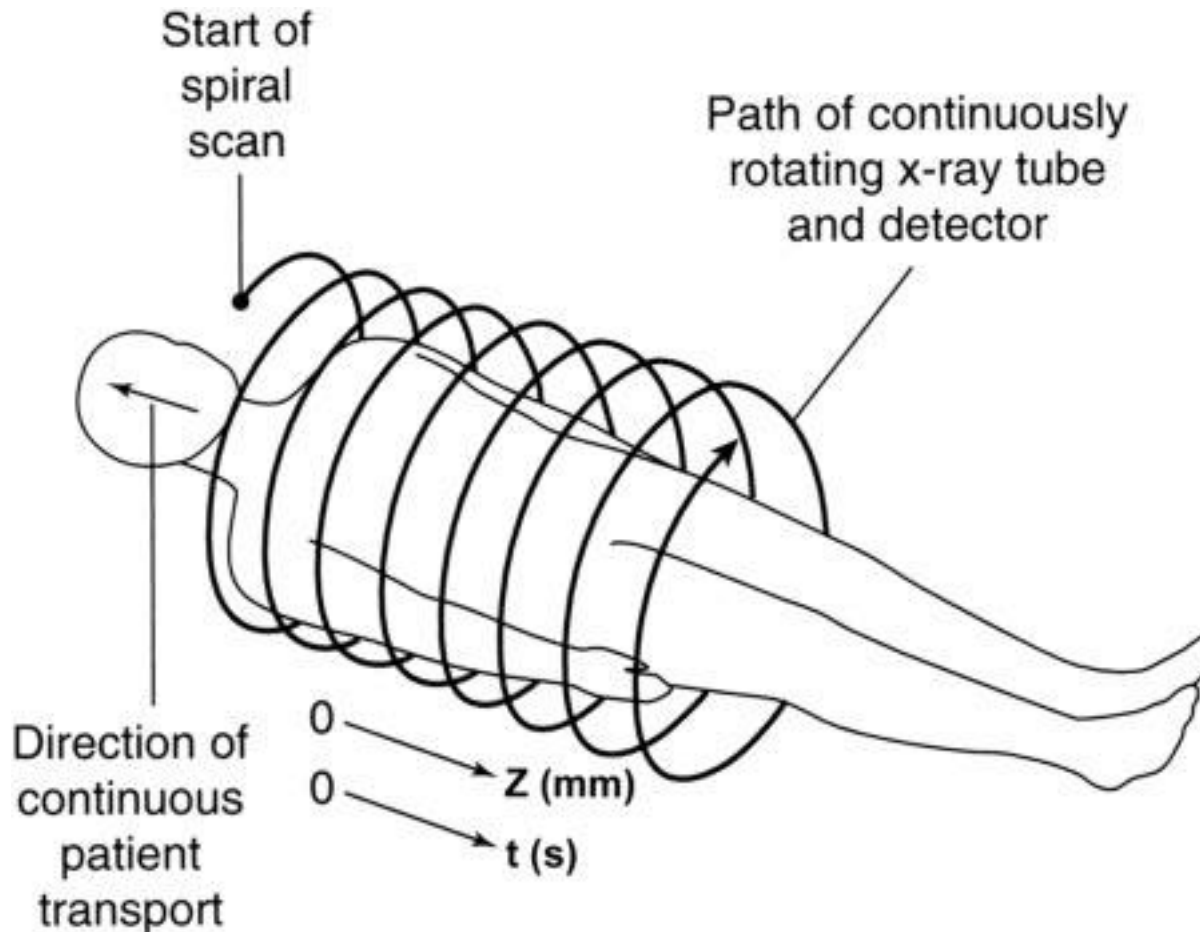
Cine CT/ millisecond CR/ultrafast CT



- Stationary-Stationary configuration – no mechanical scanning
- X ray source single tube with array of tungsten targets
- Reduced scanning time to 50ms, cardiac scanning made possible

# 6<sup>th</sup> Gen. Computed Tomography

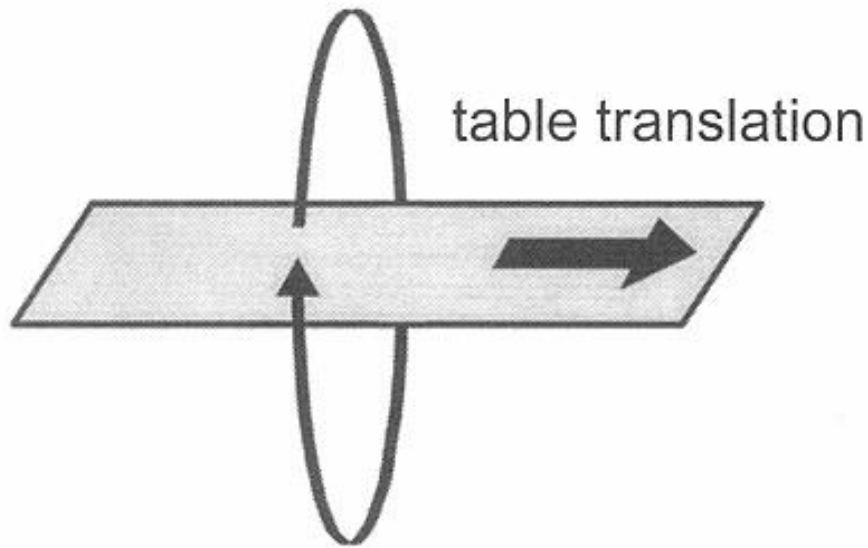
Spiral/Helical CT



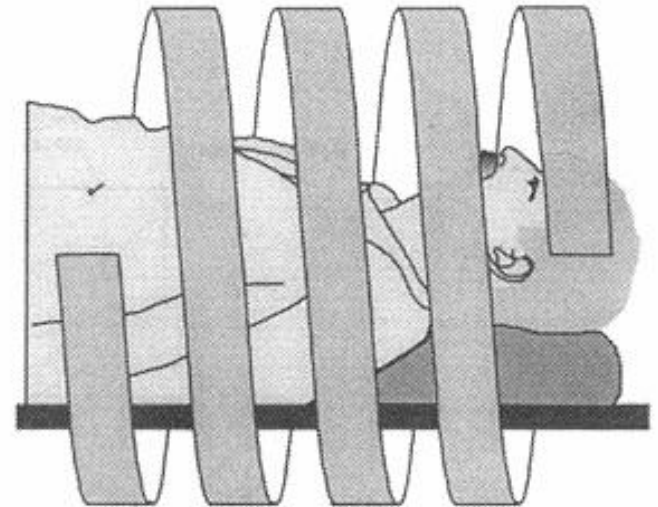
- Table translation with source rotation
- Slip ring technology X ray source continuously
- Volume data interpolation algorithms developed
- Whole abdomen in 30sec

# 6<sup>th</sup> Gen. Computed Tomography

Spiral/Helical CT



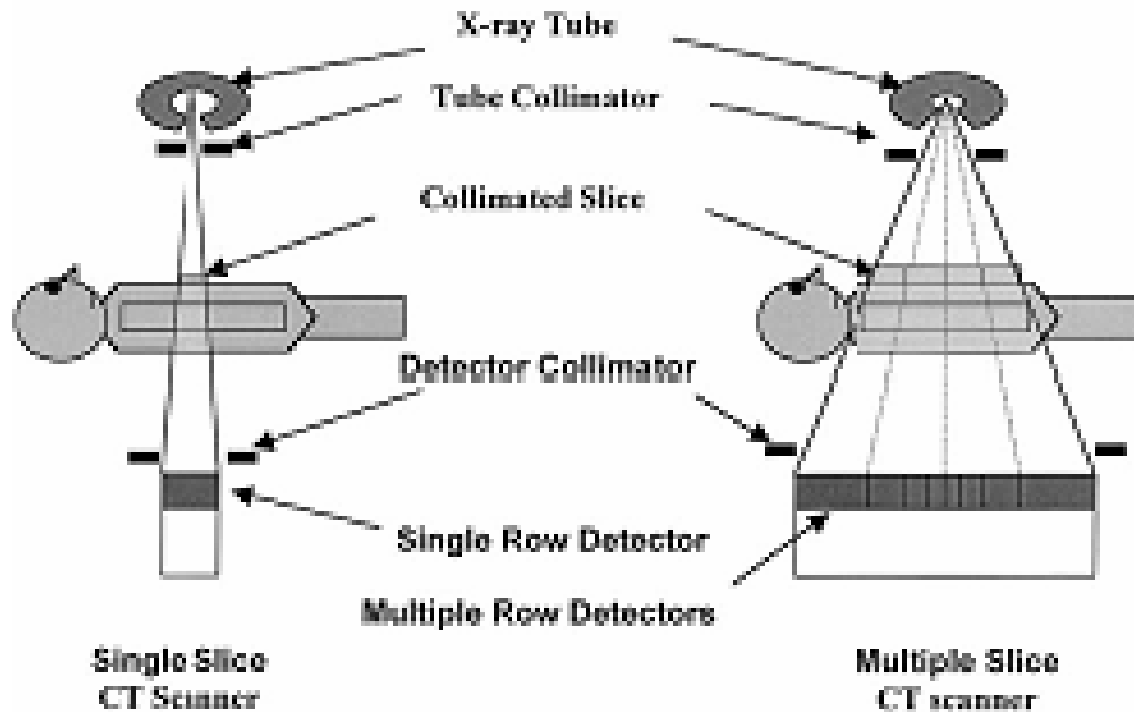
x-ray tube rotation



helical x-ray tube  
path around patient

# 7<sup>th</sup> Gen. Computed Tomography

MDCT/ Cone beam CT

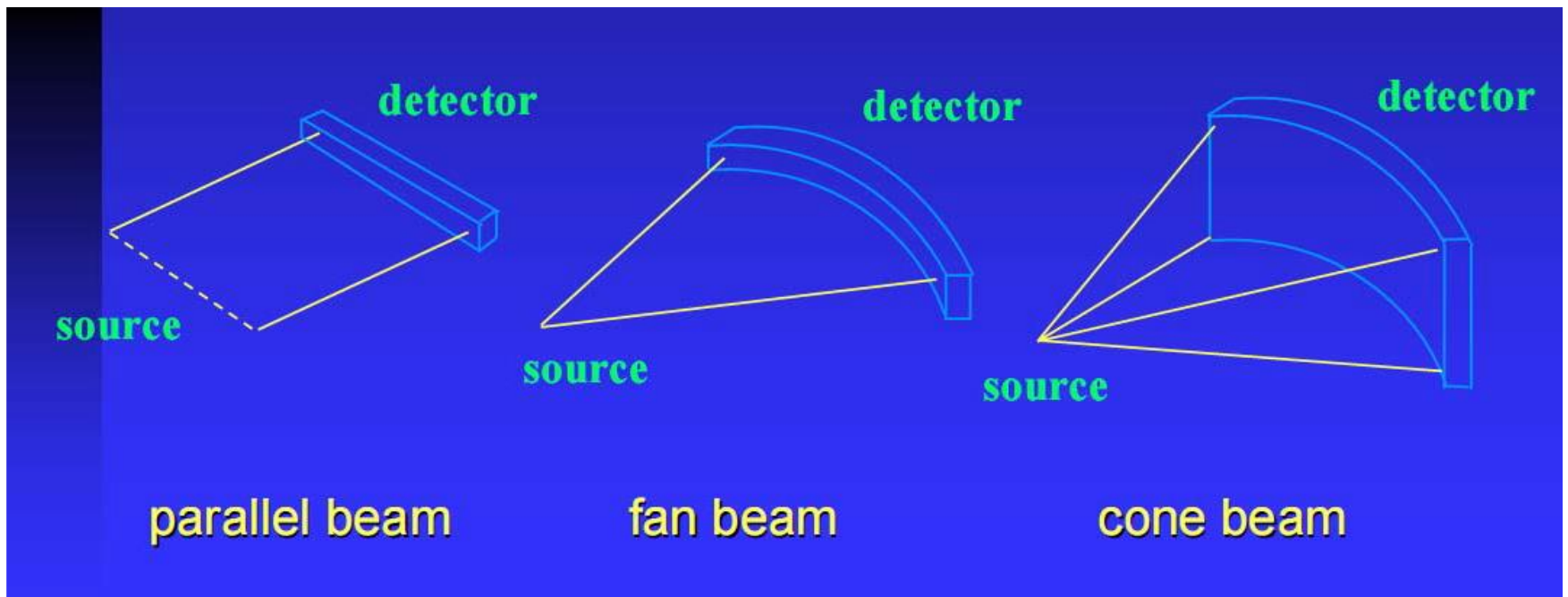


Multi-row Detector CT  
Collimator opened even more

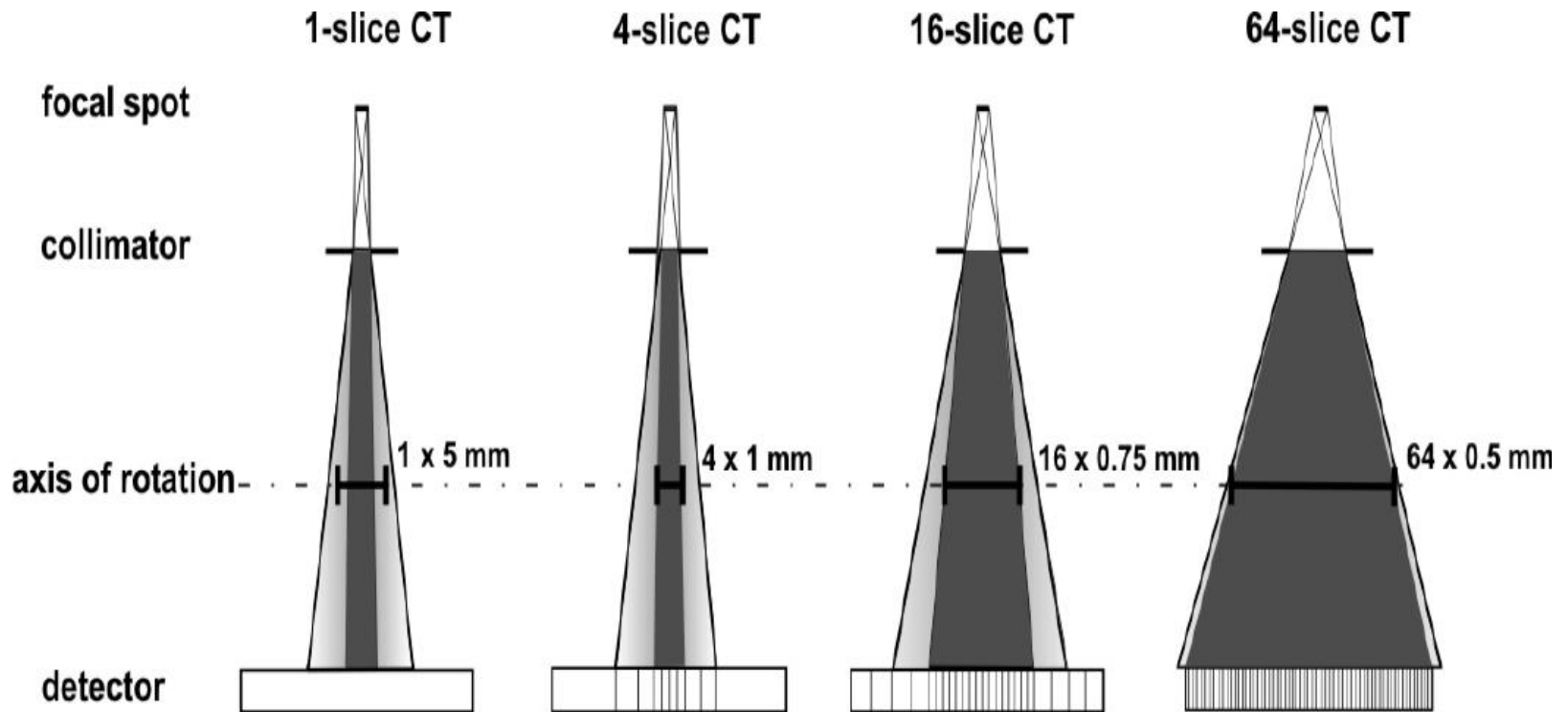
Key advance in detector technology – 2D arrays rather than one 1D array

# 7<sup>th</sup> Gen. Computed Tomography

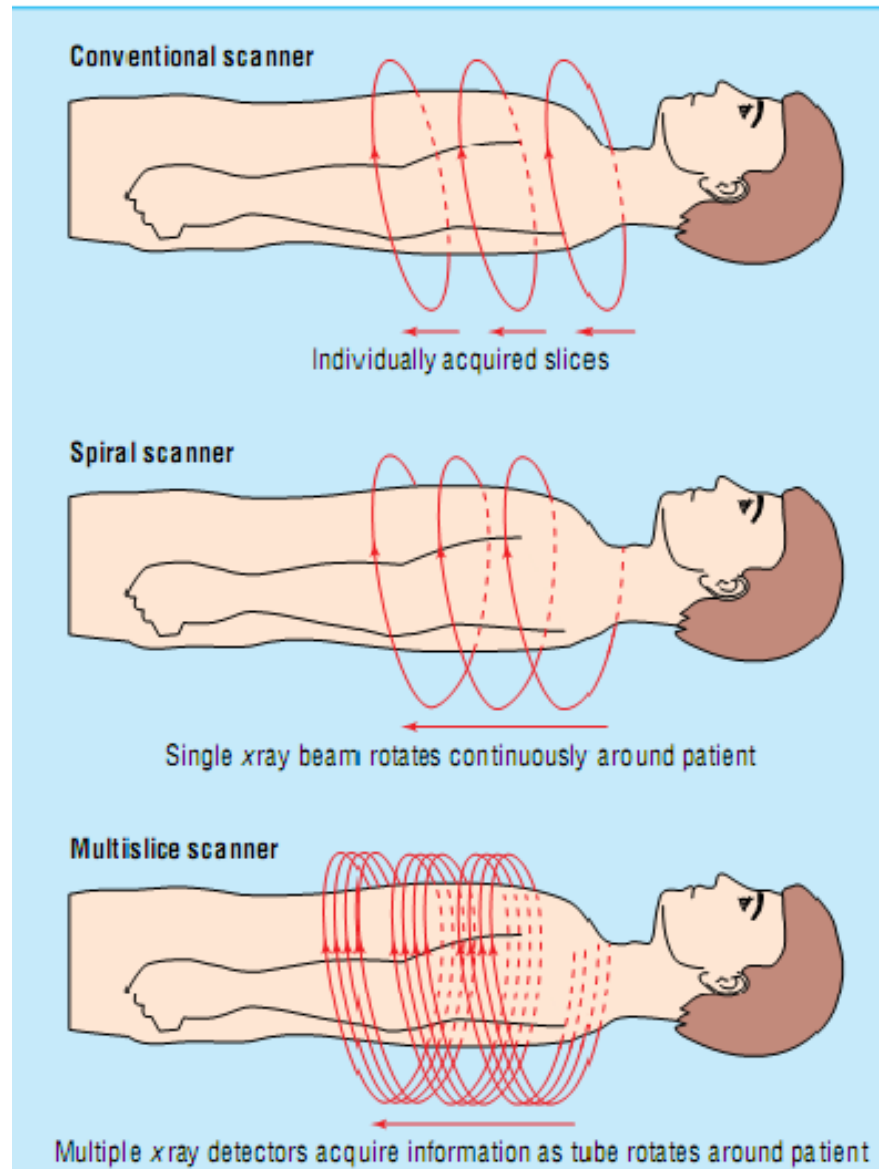
MDCT/ Cone beam CT



# War on slices!!



# 5<sup>th</sup>, 6<sup>th</sup>, 7<sup>th</sup> Gen. Computed Tomography





<b>Gen.</b>	<b>Source</b>	<b>Source Collimation</b>	<b>Detector</b>
<b>1st</b>	Single X-ray Tube	Pencil Beam	Single
<b>2nd</b>	Single X-ray Tube	Fan Beam (not enough to cover FOV)	Multiple
<b>3rd</b>	Single X-ray Tube	Fan Beam (enough to cover FOV)	Many
<b>4th</b>	Single X-ray Tube	Fan Beam covers FOV	Stationary Ring of Detectors
<b>5th</b>	Many tungsten anodes in single large tube	Fan Beam	Stationary Ring of Detectors
<b>6th</b>	3G/4G	3G/4G	3G/4G
<b>7th</b>	Single X-ray Tube	Cone Beam	Multiple array of detectors